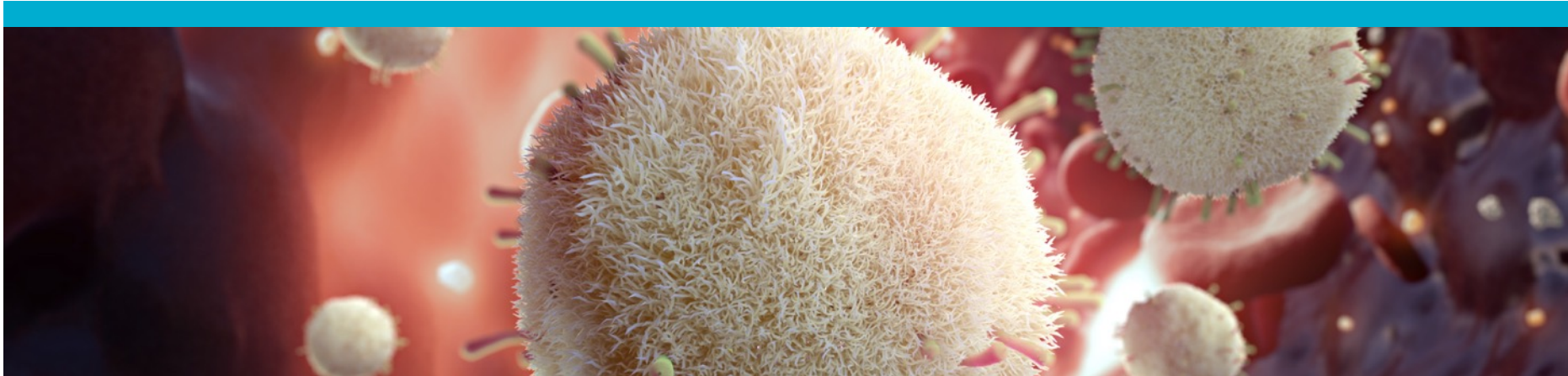


Progressing the Development of AZD2811 Nanoparticles for Intravenous Administration

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APS International PharmSci Conference

September 2019



Progressing the Development of AZD2811 Nanoparticles

Project Background

Product Development

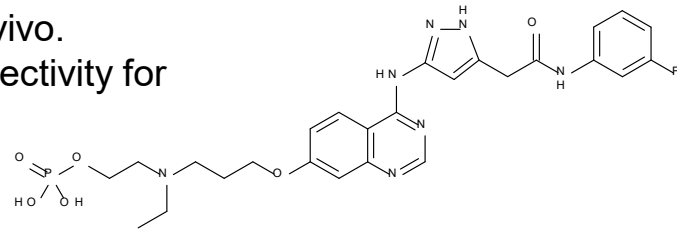
- Target product profile and potential Critical Quality Attributes
- Formulation optimisation
- Developing a robust manufacturing process
- Biopharmaceutics and potentials CQAs

Summary



Overcoming the Limitation of AZD1152 using Drug Delivery

AZD1152, a phosphate pro-drug, rapidly converts into AZD2811 in-vivo. AZD2811 is a selective AurB inhibitor with over 1000-fold higher selectivity for aurora kinase B over aurora kinase A¹



AZD1152 (barasertib, phosphate pro-drug)

AZD1152 demonstrated positive Proof of Concept in AML.

Despite this, the program was stopped due to:

- The 7-day infusion regimen limited the indications to those where patients were already hospitalised
- The dose-limiting, mechanism-related bone marrow toxicity meant that efficacious doses could only be achieved in patients with haematological cancers

These clinical limitations may be overcome by having:

- A **slow release profile** where a single infusion gives multiple days efficacious cover in an outpatient setting
- An **improved efficacy** with the potential to establish efficacious doses in solid tumour settings

1. Mortlock AA, Foote KM, Jung FH et al., *Discovery, synthesis, and in vivo activity of a new class of pyrazoloquinazolines as selective inhibitors of aurora B kinase. J Med Chem, 2007 50(9):2213-24.*

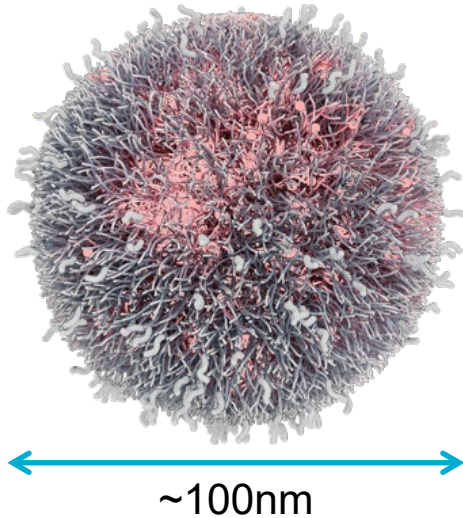
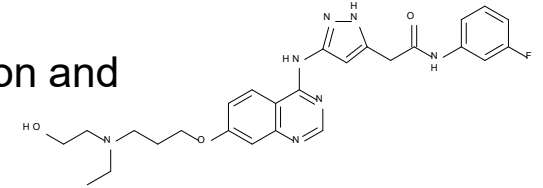


ACCURINS® Nanoparticles with Controlled Drug Release Rates

AZD2811 is encapsulated in a novel nanoparticle delivery system^{1, 2, 3}

Drug release via diffusion

Hydrophobic ion pairing with an acidic counter ion aids encapsulation and slows drug release



Controlled-Release Polymer Matrix

Poly(lactic acid) (PLA)

- FDA approved polymer
- Non-covalently entraps payload
- Regulated release of payload over days

Stealth and Protective Layer

PEG

- Hydration shell
- Protects against immune detection
- Long circulation time

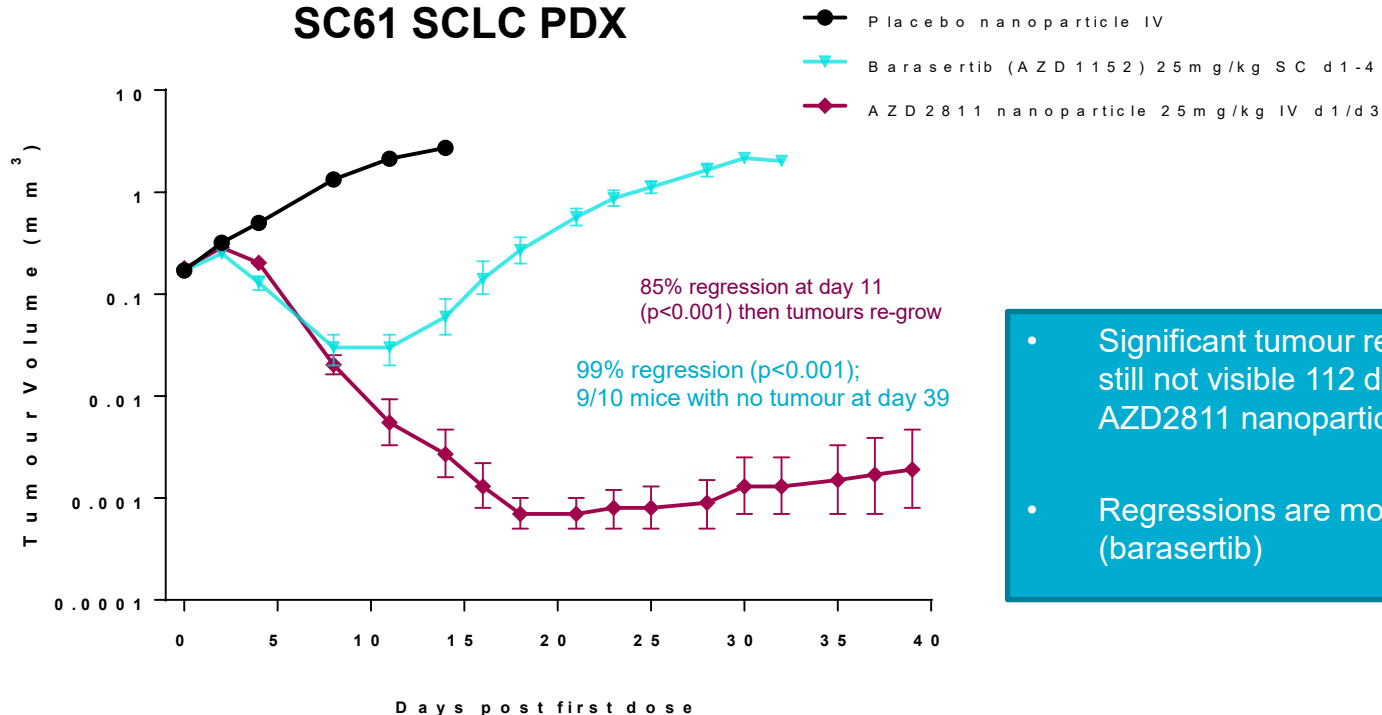
References:

1. Young HS, Shin E, Wang H, Nolan J, Low S et al. A novel in situ hydrophobic ion pairing (HIP) formulation strategy for clinical product selection of a nanoparticle drug delivery system. *J Control Release*. 2016; 229:106-119.
2. Ashton S, Taylor P, Curtis N et al. AZD1152HQPA Accurin™ nanoparticles inhibit growth of diffuse large B-cell lymphomas and small cell lung cancer. *Cancer Res*. 2015; 75:3102.
3. Ashton S, Song YH, Nolan J, Cadogan E, Murray J et al., Aurora kinase inhibitor nanoparticles target tumors with favorable therapeutic index in vivo. *Sci Transl Med* 2016; 325ra17-325ra17.



AZD2811 nanoparticle shows improved efficacy over AZD1152 at equivalent dose intensity in SCLC models

SC61 SCLC PDX



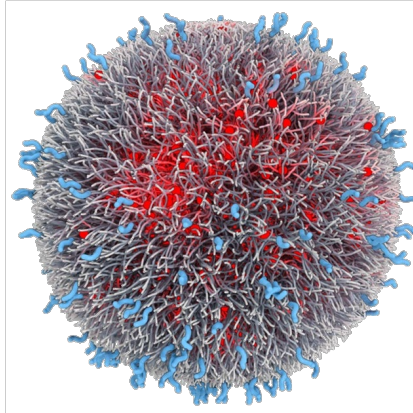
- Significant tumour regression with >80% tumours still not visible 112 days after a single cycle of AZD2811 nanoparticle
- Regressions are more durable than AZD1152 (barasertib)



Nanoparticle Target Product Profile

Physical & Chemical Composition

Release-controlling Polymer
+/- targeting ligand
Drug loading
Counter-ion
Particle size distribution
Surface charge
Drug release rate



Size: $\sim 100 \pm 30$ nm
Drug load $\sim 15\%$
Similar in vitro
Release profile



Potential Critical Quality Attributes

- Surface characteristics
- Drug Release rate/profile
- Particle size & PDI
- Morphology
- Free drug concentration

Production process

Process aids
Emulsion composition
Particle formation
Process controls (pressure, temp. etc)
Purification

Critical material attributes

Block architecture
PEG and PLA M_n
Homo-PLA, free PEG
Residual monomer, solvent

Nanoparticle Properties impact the in vivo performance, both efficacy and safety

- Biodistribution – nanoparticle circulation time and clearance, localized accumulation
- Release and clearance of drug

Formulation optimization

Formulation Optimization of AZD2811 Nanoparticle

Goals

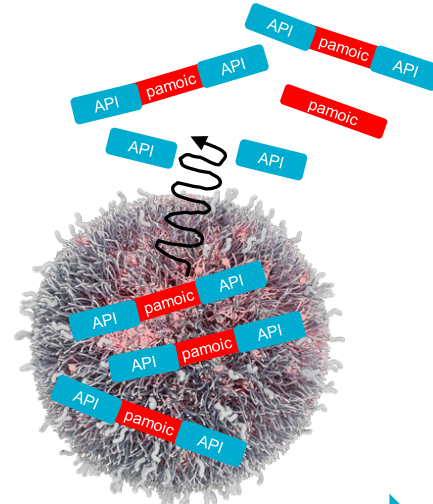
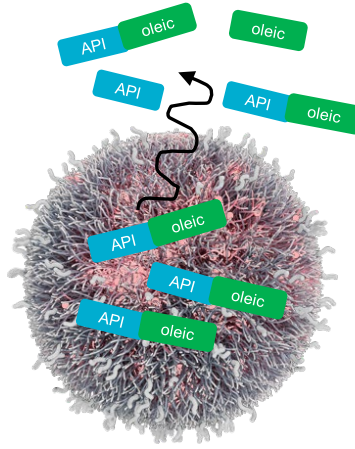
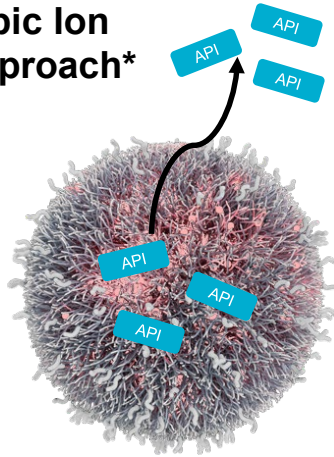
- To increase drug loading to > 12% while maintaining slow release rate
- Improve process efficiency



Benefits

- Reduced number of vials for patients
- Reduced excipient load
- Reduced development costs/cost of goods

Hydrophobic Ion Pairing Approach*



Drug loading	15%
Encapsulation Efficiency	71%
Time 50% release	120 hours

* Song et al, J Controlled Release, 2016, 229, 106

AZD2811 Drug Formulation & Product

Main Components & Function of Nanoparticle

Component	Function
AZD2811	API (~20% nanoparticle)
PLA-PEG	Hydrophobic PLA (16kDa) to control release Hydrophilic PEG (5kDa) as stealth layer
Pamoic Acid	Functional excipient, forms hydrophobic ion pair with API AZD2811:Pamoic 1:0.5

- Presented as a frozen suspension for Ph1 & 2
- Lyophile will be investigated for commercial product



A novel *in situ* hydrophobic ion pairing (HIP) formulation strategy for clinical product selection of a nanoparticle drug delivery system

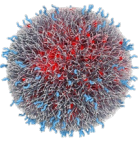
Young Ho Song^a, Eyoung Shin^a, Hong Wang^a, Jim Nolan^a, Susan Low^a, Donald Parsons^a, Stephen Zale^a, Susan Ashton^b, Marianne Ashford^c, Mir Ali^a, Daniel Thrasher^a, Nicholas Boylan^a, Greg Troiano^{a,*}

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Developing a robust manufacturing process

Manufacturing Process for AZD2811 nanoparticle

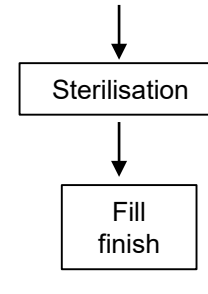
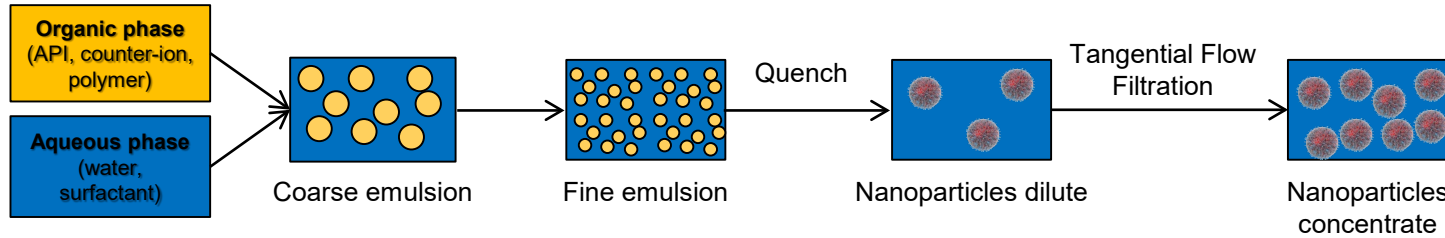


Target Attributes



Size: $\sim 100 \pm 30$ nm
Drug Load: $\sim 20\%$

Similar *In vitro* release profile



$$d_{max} = \epsilon^{-2/5} \gamma^{3/5} p^{-1/5}$$

Energy density Surface tension Laplace pressure

The shear stress applied by the process must exceed the Laplace pressure, which is inversely proportional to droplet diameter

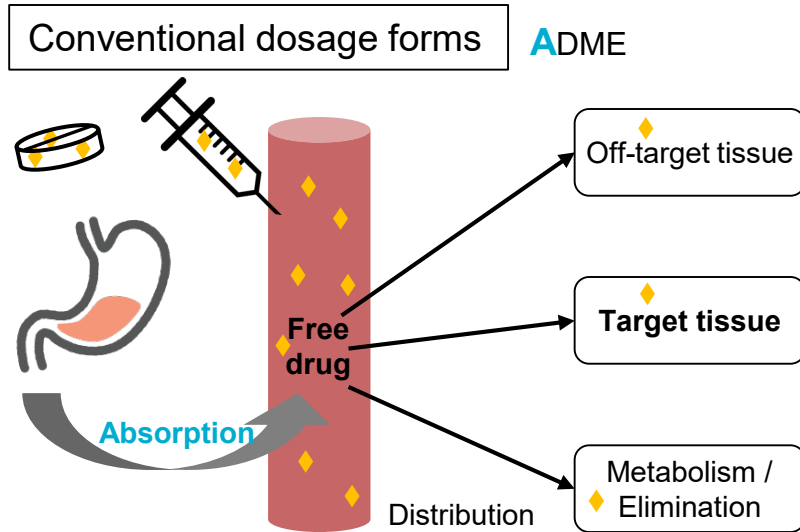


Nanoparticle Manufacturing Process Control Aspects

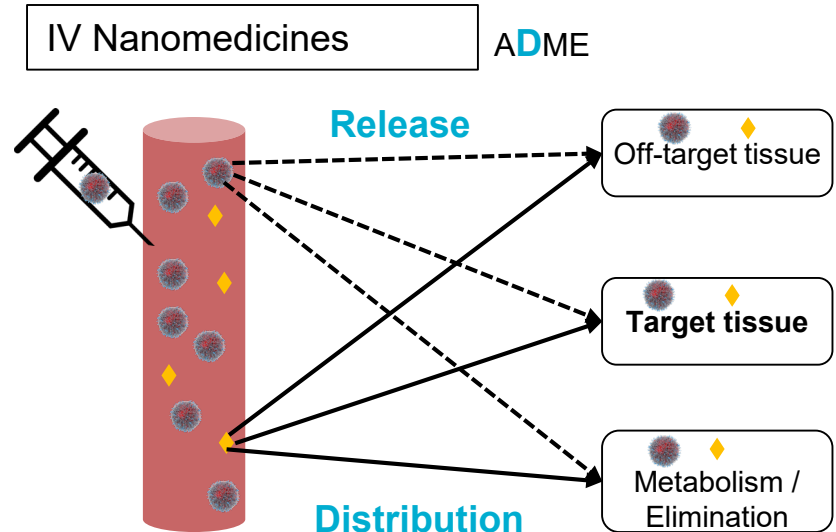
Process Step	Input Parameters	Key Outputs	Impact
Coarse Emulsification	Surfactant quantity Energy Temperature Phase viscosities	Droplet size distribution Emulsion stability	Increasing energy input → smaller droplets Decreasing surface tension (more surfactant) → smaller droplets Smaller droplets → Increased Laplace pressure Increasing temperature → less stable emulsion & bigger droplets
Fine Emulsification	Surfactant quantity Energy Temperature Phase viscosities	Droplet size distribution Emulsion stability Drug loading Drug release rate	Decreasing surface tension → smaller droplets Smaller droplets → Increased Laplace pressure Increasing temperature → less stable emulsion, reduced drug loading
Droplet stabilisation	Energy Time Sink conditions Temperature/ Pressure	Droplet size distribution Drug loading Drug release rate	Temperature / pressure affects residual solvents, drug loading Rate of solvent removal impacts drug loading, residual solvents
Clean & concentrate particles	Diavolumes Transmembrane pressure Flow rate Concentration	Free drug content Solvent content Drug loading Concentration / Assay	More diavolumes → reduced solvent / free drug concentration, longer processing times and waste Need to optimise transmembrane pressure, concentration, flow rate, temp & diavolumes

Biopharmaceutics and potential CQAs

Biopharmaceutics of AZD2811



- Efficacy/safety driven by systemic exposure = plasma conc profile of **free drug**
(target and off-target tissue concs in eqm with plasma conc)
- Plasma concentration limited by drug **absorption**
(unless IV)
 - ➔ **API solubility/permeability, drug product dissolution**

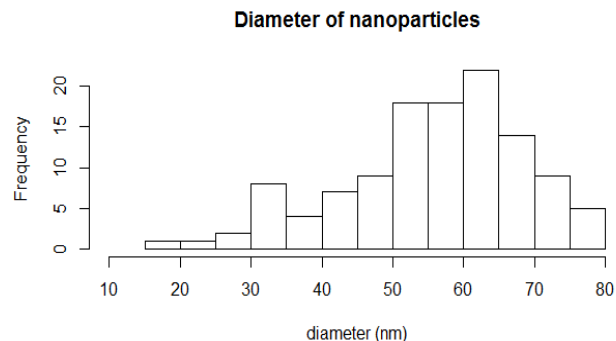
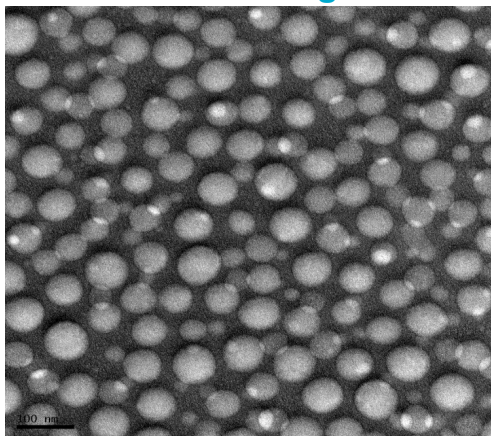


- Systemic exposure: 2 entities present **released drug AND encapsulated drug**
- Different distribution patterns ➔ target exposure no longer driven **only** by plasma conc ➔ **Focus on NP attributes that can impact release and distribution**



Particle Sizing of Nanoparticles

Particle size using Transmission Electron Microscope (TEM)



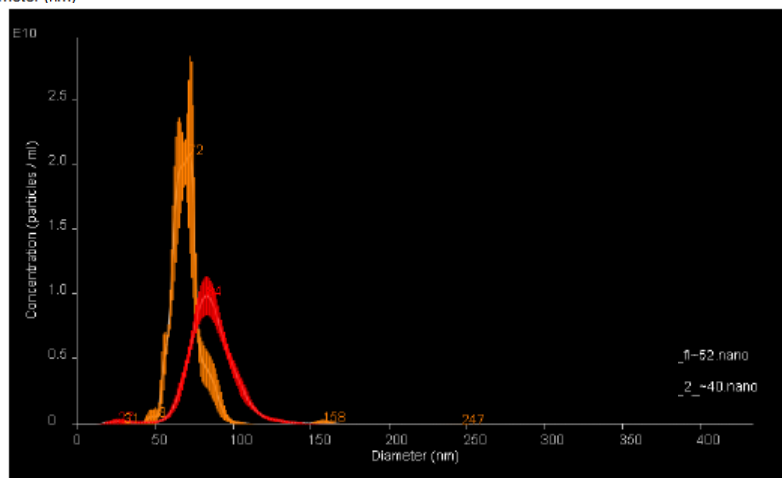
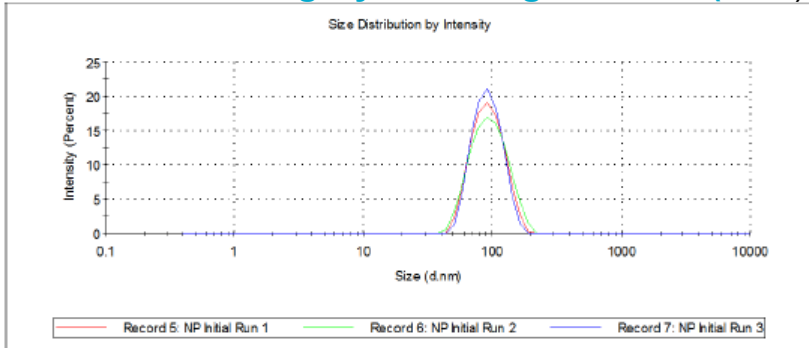
Mean: 57 nm

Standard deviation: 13 nm

Range: 18 – 80 nm

Average size of nanoparticles (based on measurement of 118 nanoparticles):

Particle size using Dynamic Light Scatter(DLS)



Scatter

Mode: 67.8 nm

Mean: 70.3 nm

Total concentration: 4.08×10^{11} particles/mL

Fluorescence:

Mode: 86.4 nm

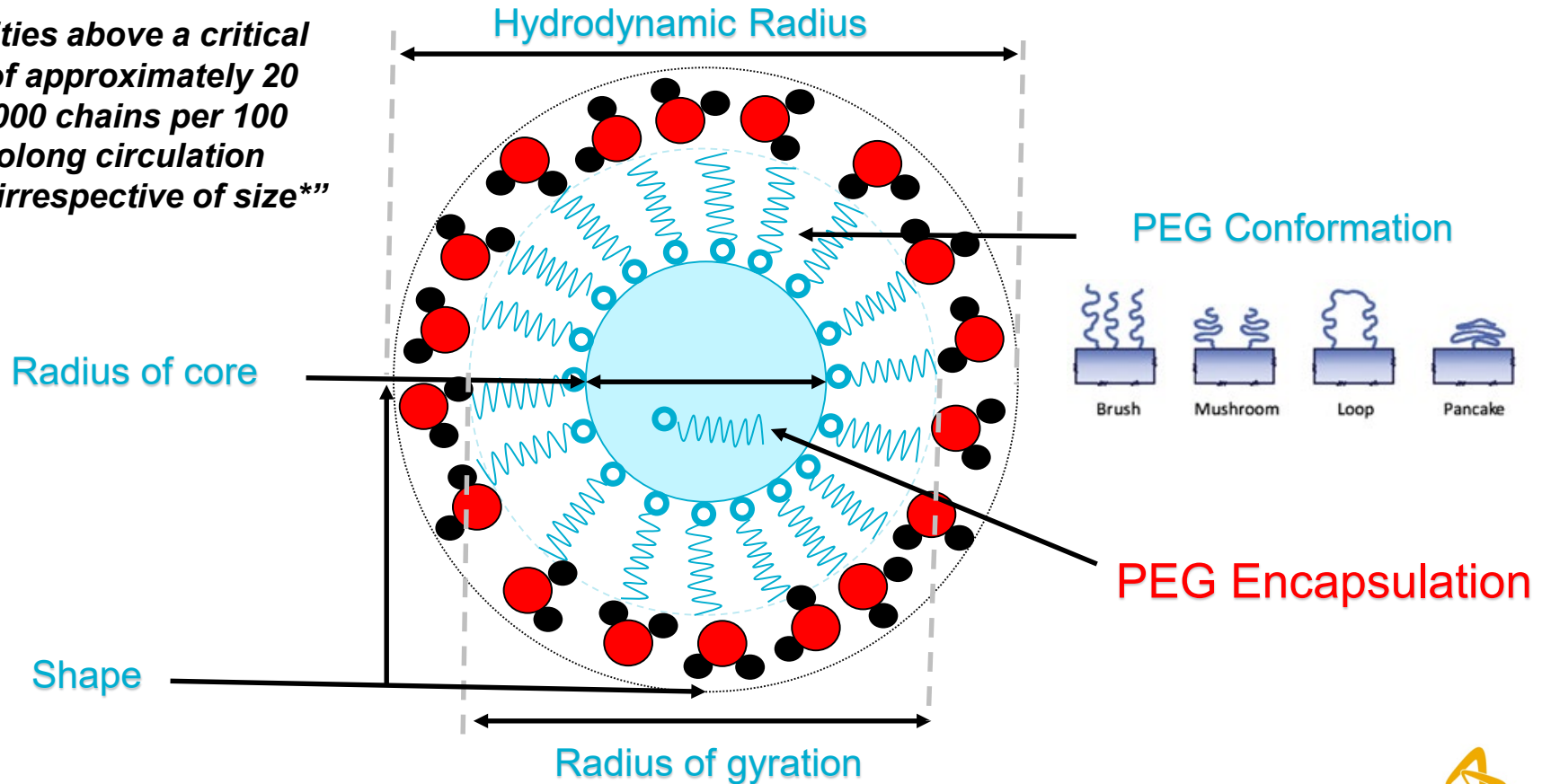
Mean: 85.8 nm

Total concentration: 3.05×10^{11} particles/mL

Particle size using nanoparticle Tracking Analysis (NTA)

Stealth Layer Analysis- Quality and In Vivo performance

“Densities above a critical value of approximately 20 PEG-5000 chains per 100 nm² prolong circulation times, irrespective of size”*

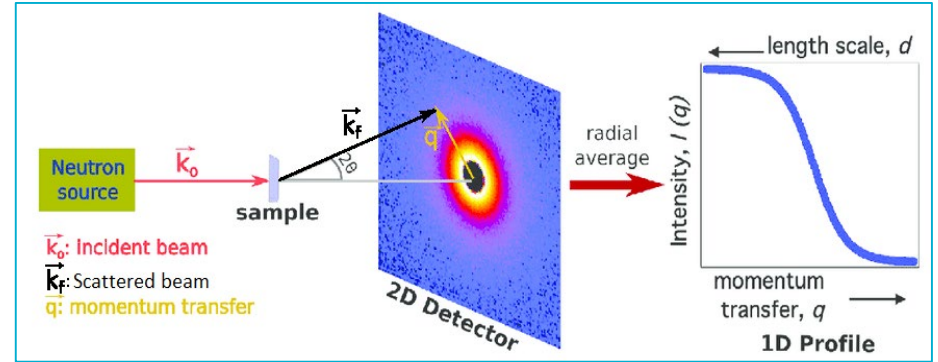


*Bertrand et al, Mechanistic understanding of in vivo protein corona formation on polymeric nanoparticles and impact on pharmacokinetics, Nat. Comm, 2017, 8, 777



Stealth Layer Characterisation

- Surface PEG quantification with NMR
 - Quantify total PEG in/on nanoparticle
 - Quantify PEG in nanoparticle
 - Subtraction = PEG on surface
- Determine size (R_g) via SANs and therefore surface area
- Packing density: PEG/ 100 nm²

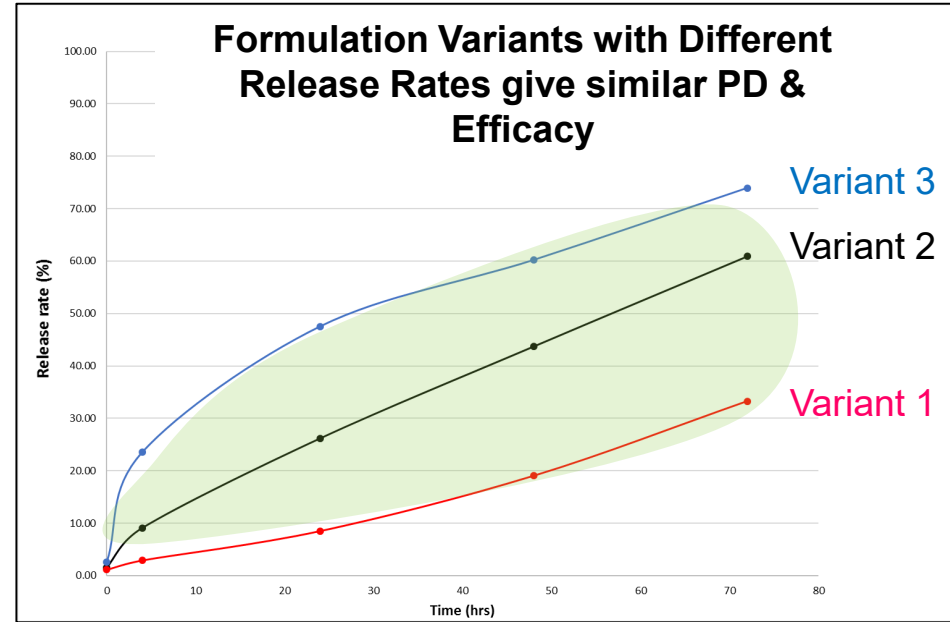


Neutron Scattering



Further work to support Product Development

- Identify CQAs and define acceptable drug product attribute ranges to ensure equivalent performance across clinical batches
- Define a robust, biorelevant, discriminatory IVR (in-vitro release) method and assess in-vitro in-vivo correlation
- Process scale up to commercial scale



In Summary

- AZD2811 is progressing through Phase I/II
- Significant progress in understanding the physical and chemical composition of the nanoparticles
- Robust clinical product manufacturing process
- Sound understanding of process parameters that will aid commercial process optimisation
- Further work on-going to optimise the in-vitro in-vivo release correlation for product commercialisation



Acknowledgements

- Many many colleagues working in the nanomedicines field in AstraZeneca Pharmaceutical Sciences, Oncology and Pharmaceutical Technology and Development groups
- AZD2811 Project Team and sub teams
- External collaborators in particular those from ex BIND Therapeutics, University of Warwick and ISIS.

